

Spatiotemporal Modeling for Image Time Series with Appearance Change: Application to Early Brain Development

James Fishbaugh, Martin Styner, ..., Guido Gerig

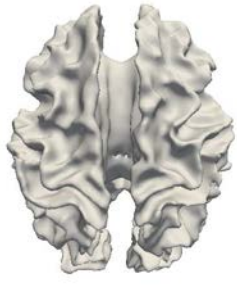
MICCAI 2019, MFCA workshop, to appear Oct. 2019, LNCS Springer Verlag



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Previous Work: Shape regression from discrete time points



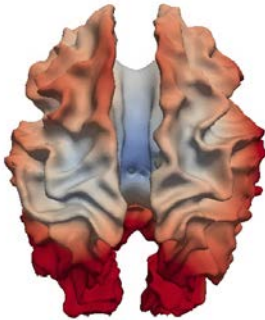
6 month



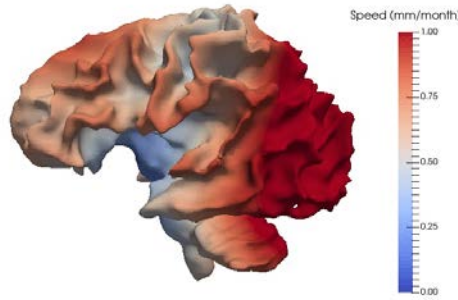
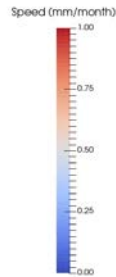
12 month



24 month



6.00 months



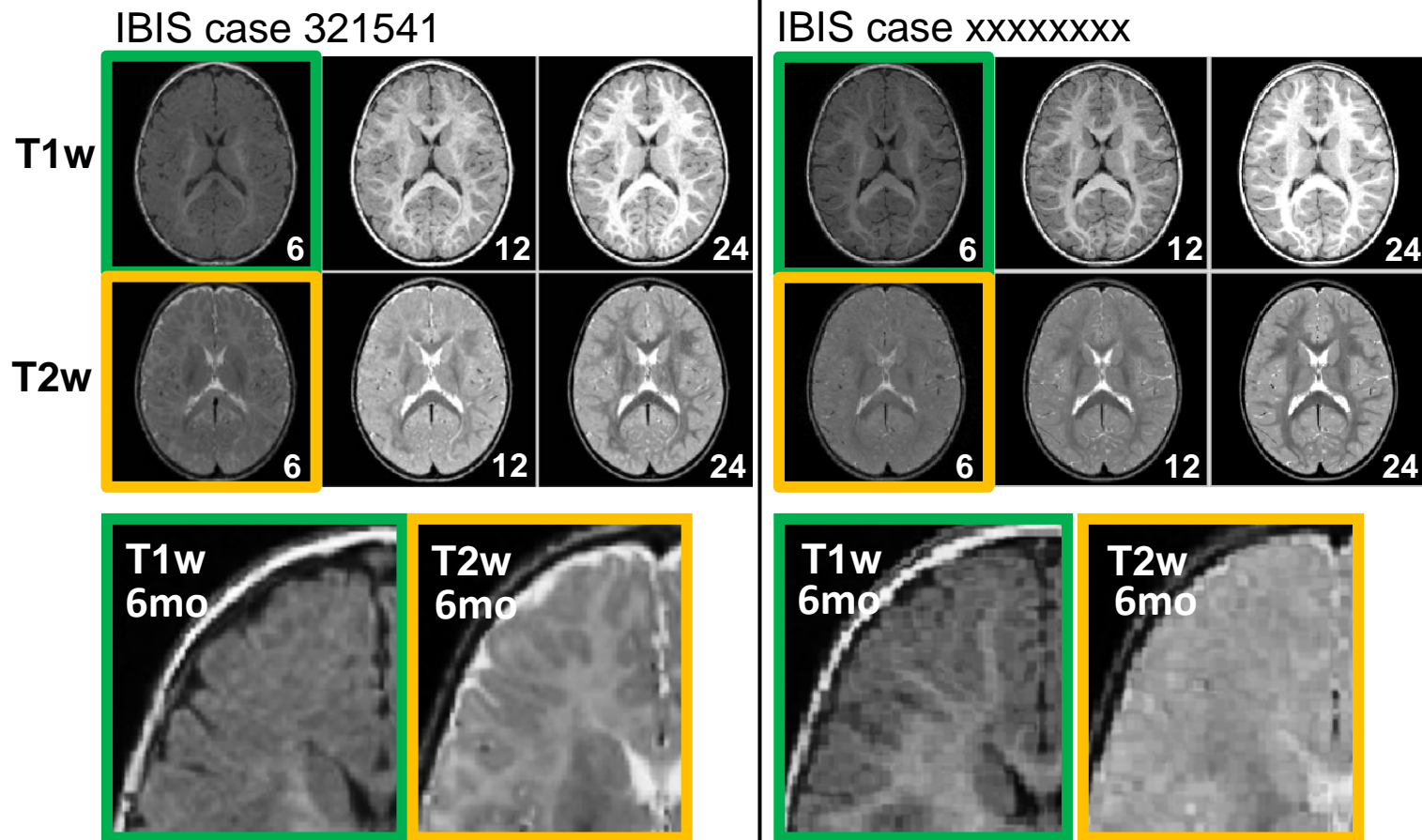
6.00 months

Geodesic Shape

Regression: Growth of brain surface color-coded with local speed. Please notice rapid early development of occipital lobe (back of brain, dark red) due to early visual cortex maturation.

Fishbaugh et al., *MedIA Elsevier* 2017 / *ISBI* 2018

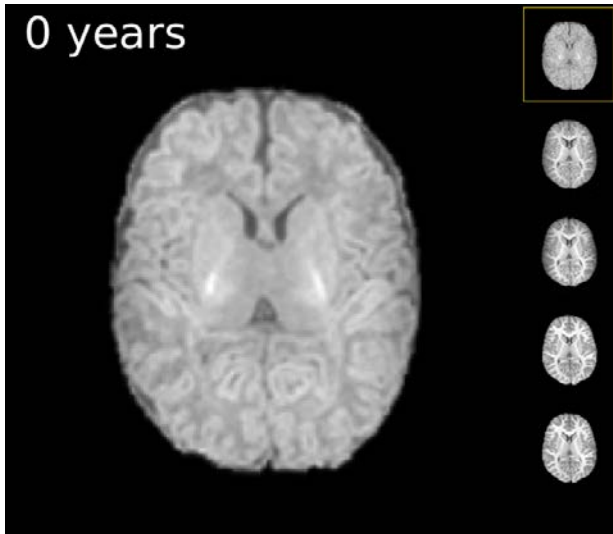
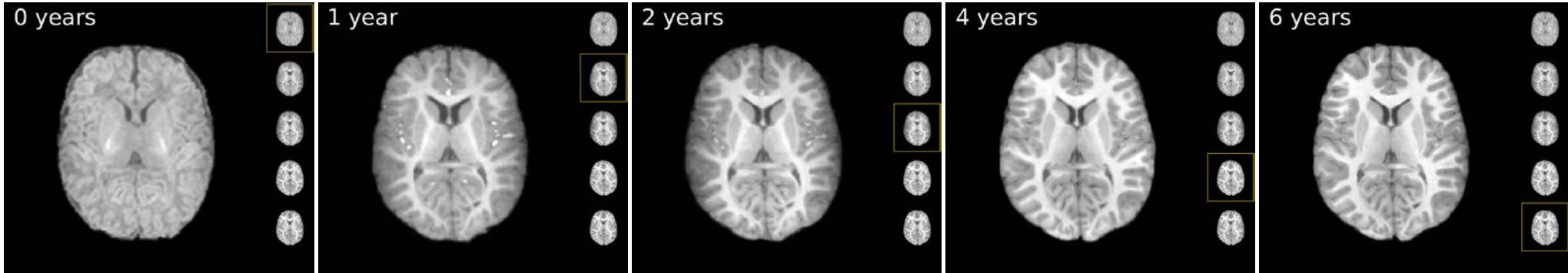
Motivation: “Growth/Maturation” seems also encoded in multi-modal MRI contrast



Observation: Two IBIS cases show different T1w/T2w contrast changes with different time trajectories.

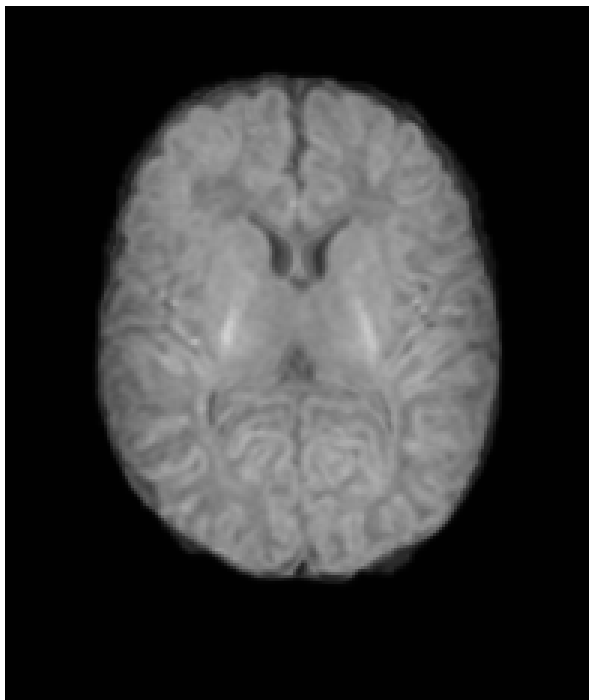
Vardhan & IBIS et al.,
MICCAI 2017

New: Regression of Structure & Appearance

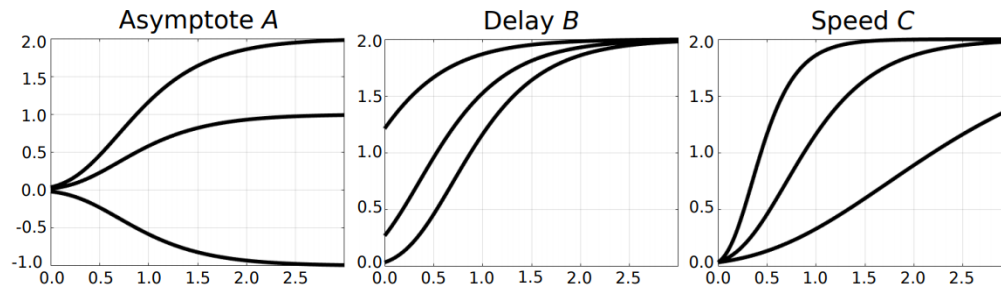


Challenges and Motivation:

- **MRI represents anatomy & contrast.**
- Co-registration of images with very different, locally varying contrasts is challenging.
- New approach: Joint modeling of growth trajectories of structure and appearance.

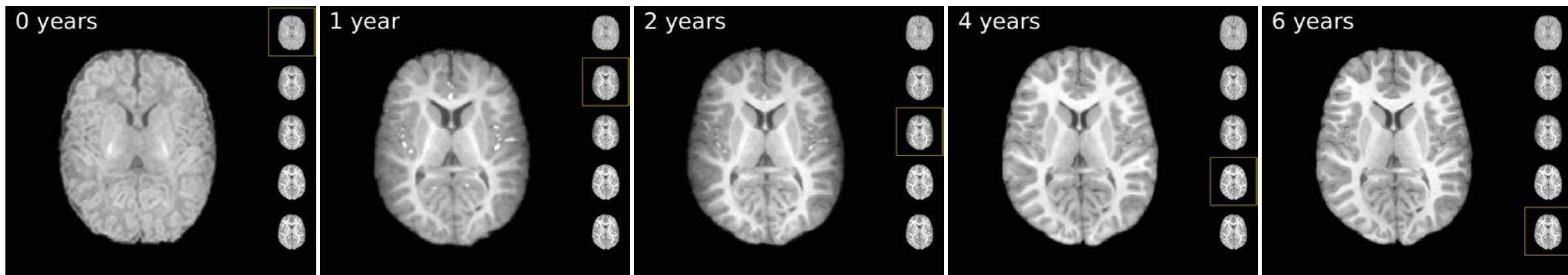


Spatiotemporal Model With Appearance Change



Gompertz
model for
intensity
(Sadeghi,
ISBI'13)

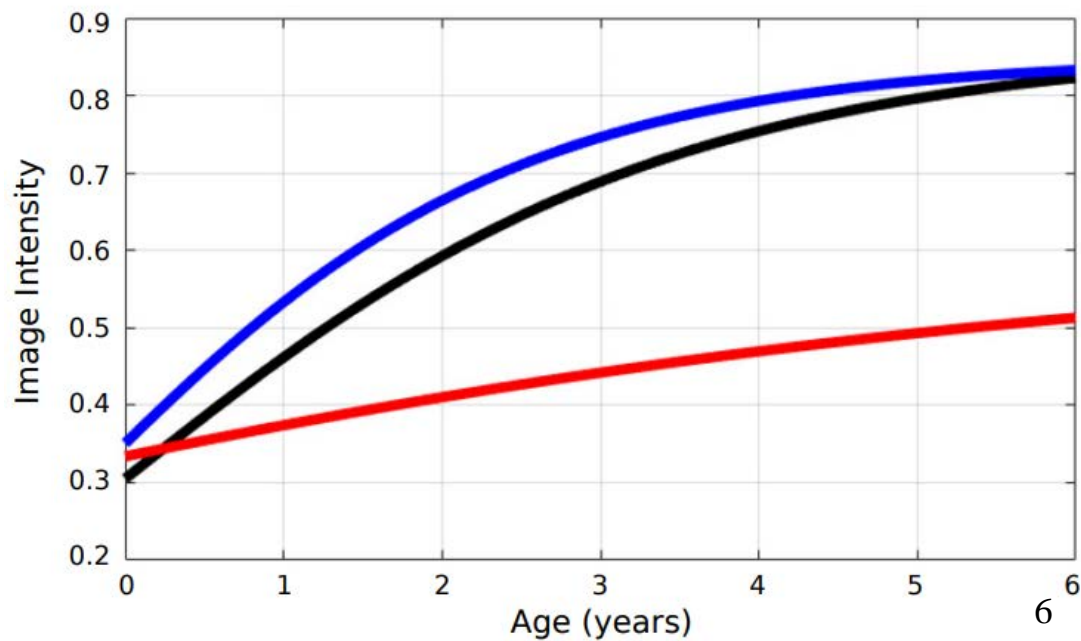
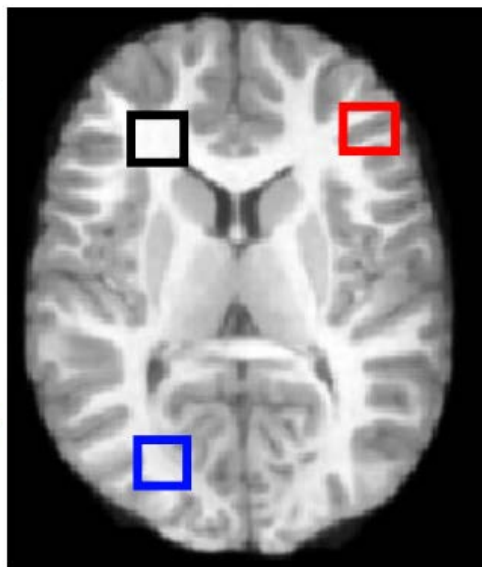
$$E(\alpha(t), \mathbf{c}_0, A, B, C) = \left[\sum_{i=1}^{N_{obs}} \lambda_D d(\phi_{t_i}(\hat{\mathbf{I}}(t_0)), I_{t_i})^2 + \lambda_A d(\hat{\mathbf{I}}(t_i), I_{t_i})^2 \right] + \lambda_R \int_{t_0}^T \|\mathbf{a}(t)\|_V^2 dt + \lambda_{TV} \text{TV}(A, B, C)$$

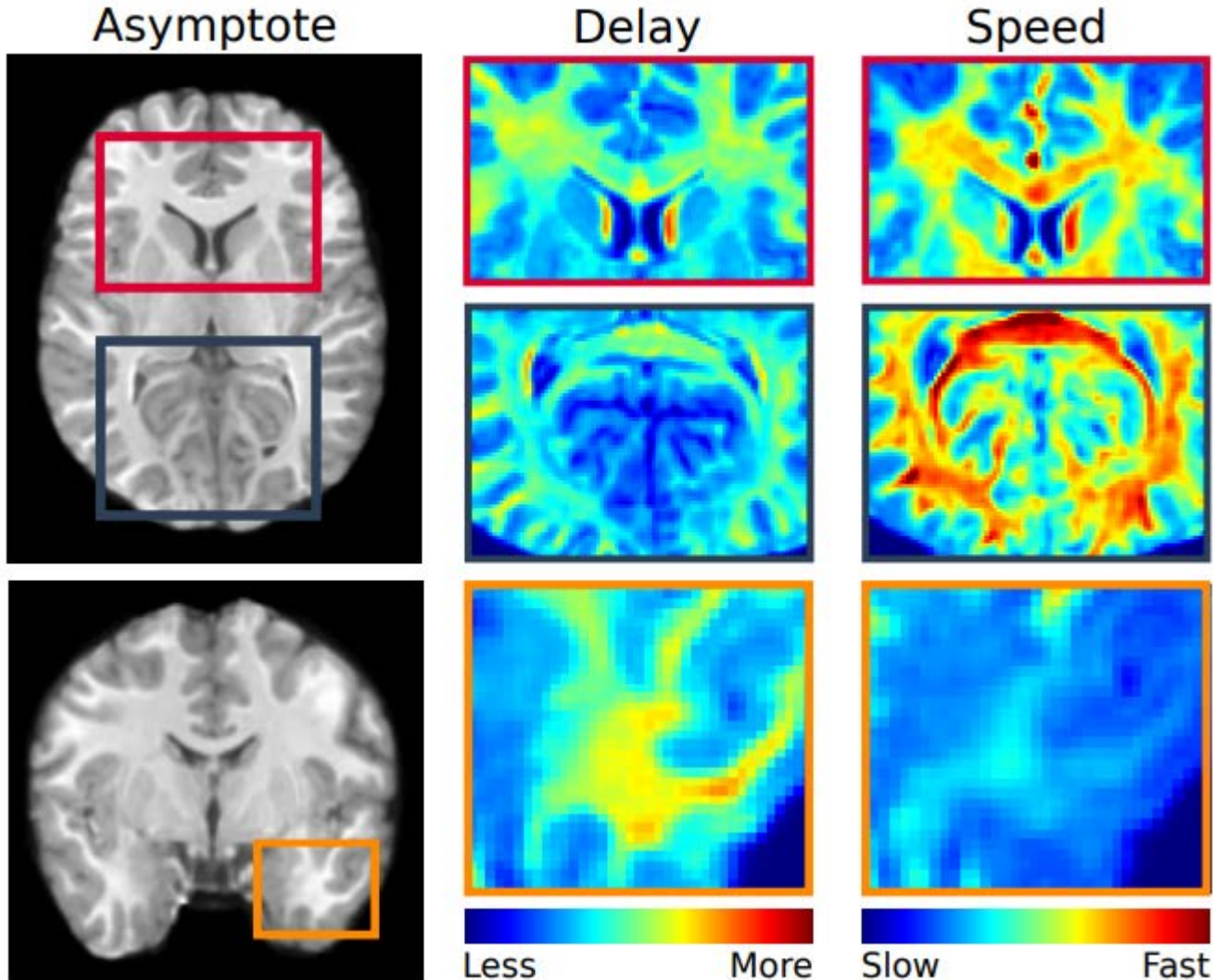


White Matter
(Anterior)

Grey Matter

White Matter
(Posterior)

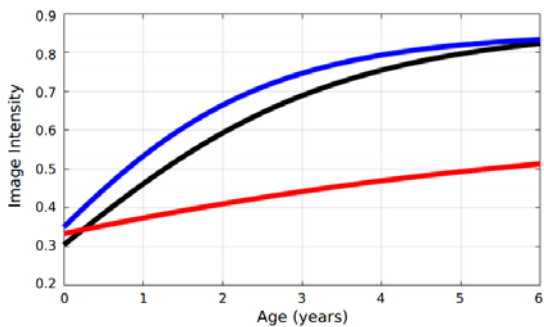




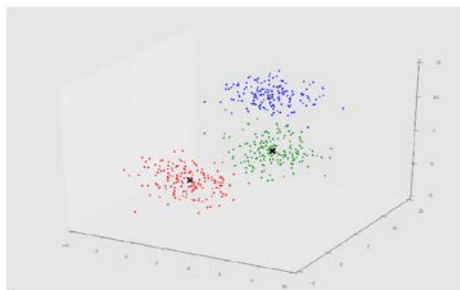
Appearance model provides additional information on tissue maturation:

- GM and WM show very different trajectories.
- Frontal, occipital and temporal lobes differ in delay and speed.

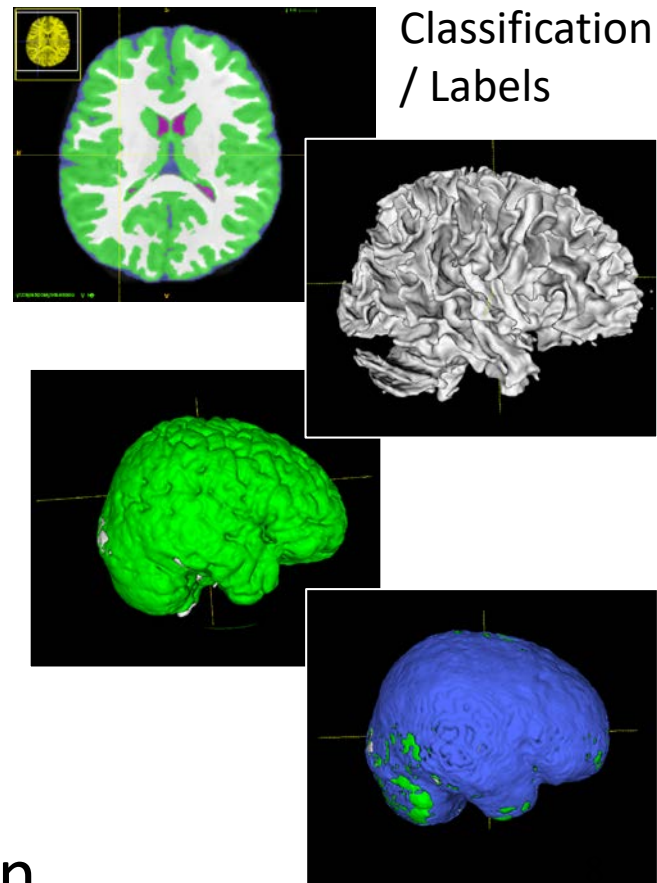
Data-driven segmentation



Voxel-wise appearance change



Clustering in A,B,C



Classification / Labels

Work in progress:

Towards fully data-driven tissue segmentation



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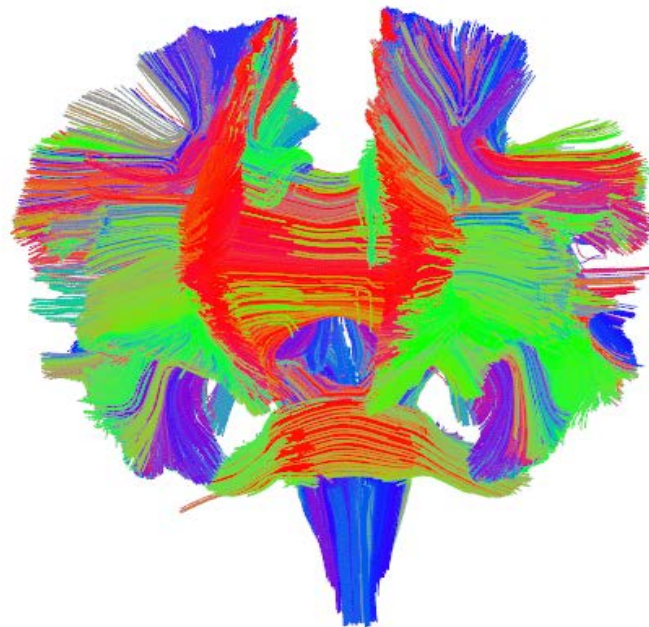
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A framework to construct a longitudinal DW-MRI infant atlas based on mixed effects modeling of dODF coefficients

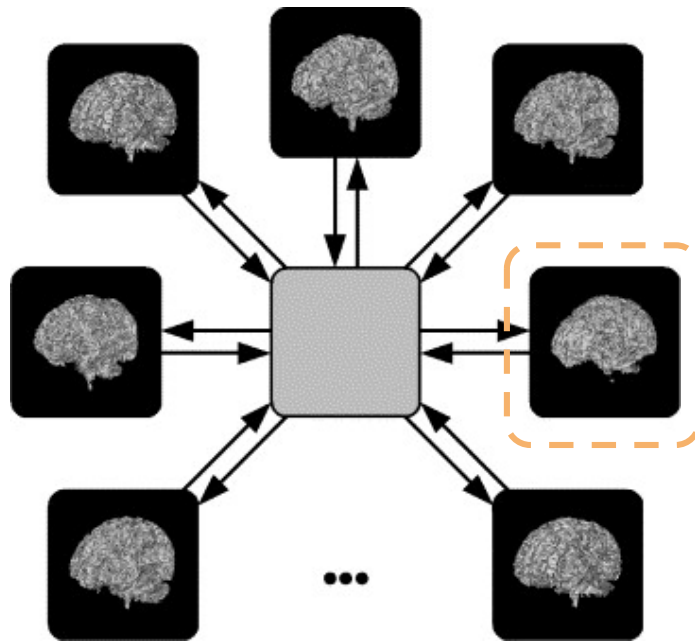
Heejong Kim, Martin Styner, Joseph Piven, and Guido Gerig

MICCAI CDMRI workshop, Oct. 2019

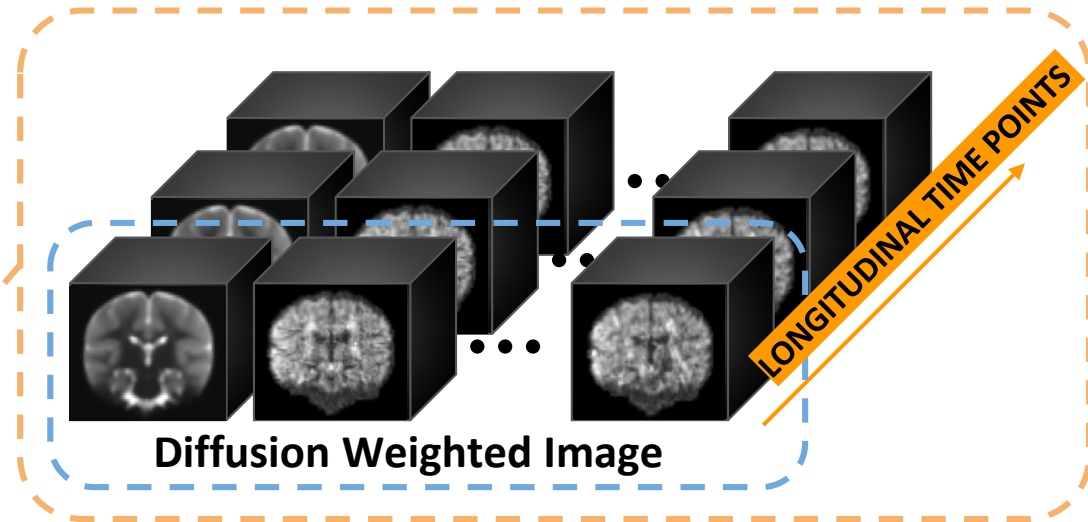


003 months

Goal: Framework to construct a *continuous* longitudinal DW-MRI infant atlas



Atlas construction framework
on structural brain image*

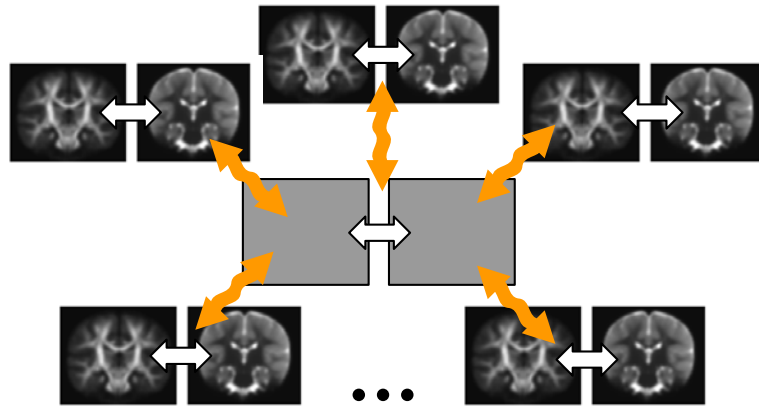


Diffusion Weighted Image

- Atlas building on longitudinal DW images is even more challenging because of **time changes**.

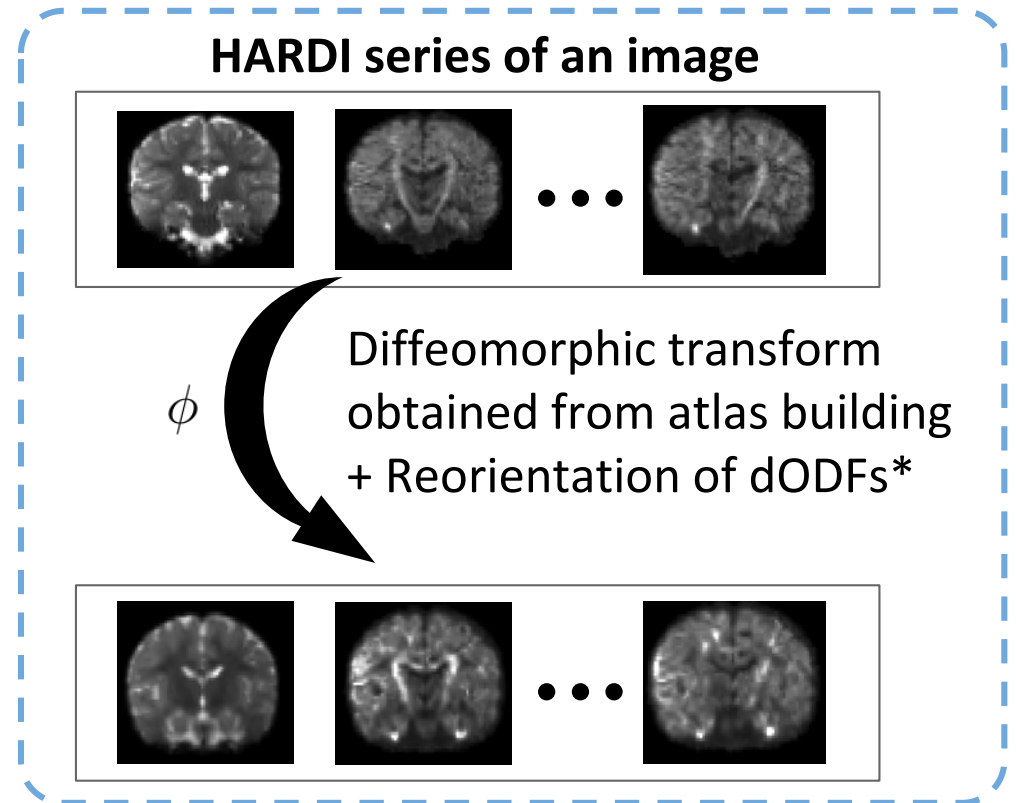
→ **Goal:** Propose a framework to construct a continuous longitudinal DW-MRI infant atlas

Atlas Building Steps



Multivariate atlas construction framework (B0, FA)

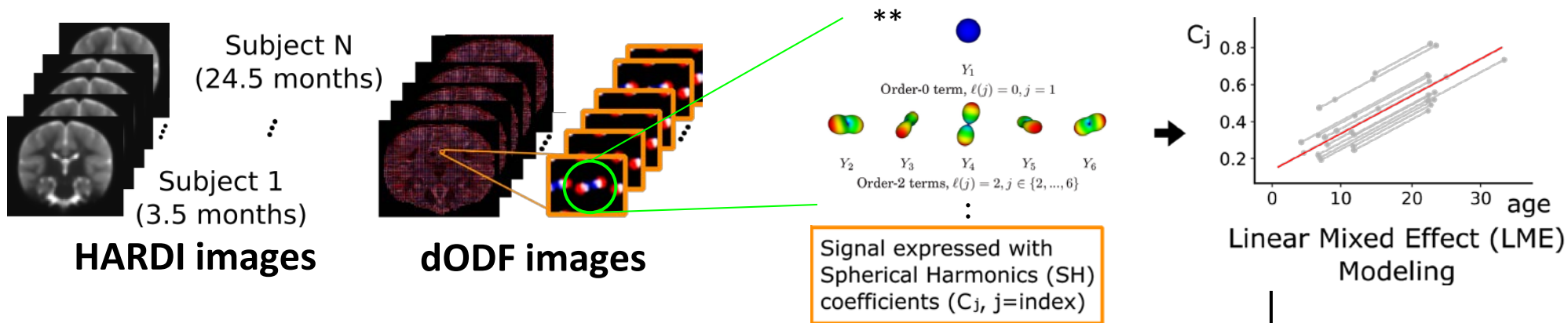
1) Calculating nonlinear deformation of each subject into atlas space.



2) Mapping reoriented diffusion maps into atlas space.

*Yap, et al., IEEE transactions on medical imaging (2012)

Longitudinal dODF atlas construction



- Analytical q-ball based diffusion orientation distribution function (dODF)* calculated for each voxel.†
- LME model for spherical harmonics (SH) coefficients for the population of subjects and repeated measures over time.

$$c_j \sim X\beta + Z\alpha + \epsilon,$$

β = a fixed effects vector \longrightarrow **Age**
 $X = [1, t]$
 α = a random effects coefficient \longrightarrow **Subject**
 Z = a design matrix
 ϵ = errors

*Descoteaux, Magnetic Resonance in Medicine, 2007

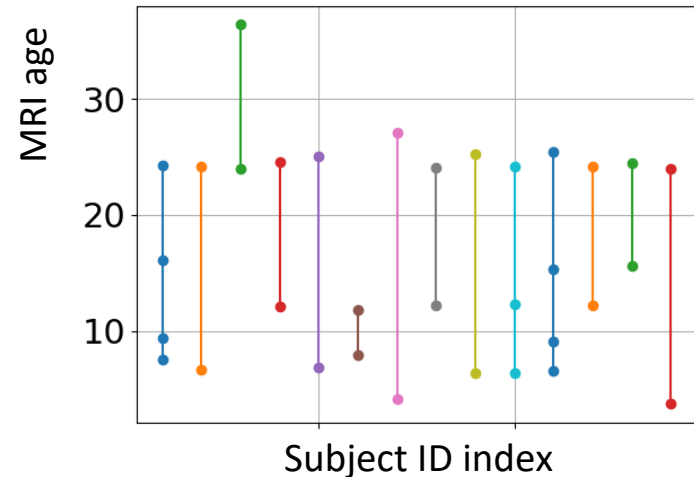
**Descoteaux, High Angular Resolution Diffusion MRI: from Local Estimation to Segmentation and Tractography, 2010

† J Jiang, Linear and generalized linear mixed models and their applications, 2007

RESULT: ACE-IBIS* Clinical Data



- Autism infant imaging project (ACE-IBIS)
- HARDI 64dir from 3-T Siemens TIM Trio Scanners
- Quality control techniques include DTIPrep** and Q-space resampling[†]
- Longitudinal study 3- to 36- month
 - 33 images from 14 healthy infants

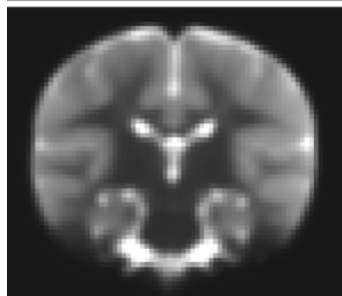


*Autism Centers of Excellence Infant Brain Imaging Study

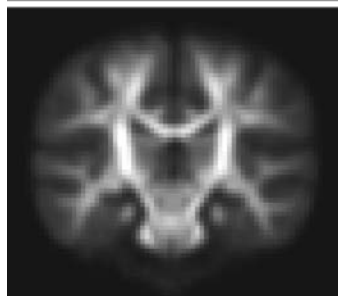
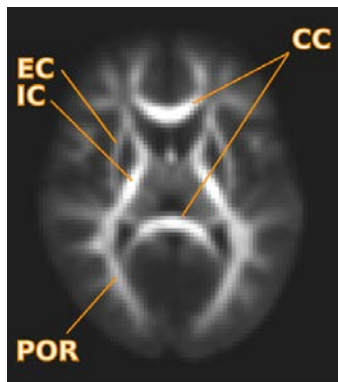
**Oguz et al., Front. In Neuroinformatics, 2014

† Elhabian et al., ISBI, 2016

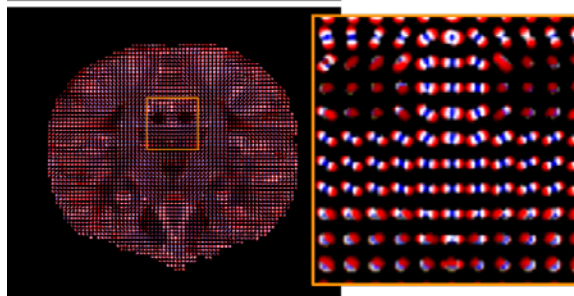
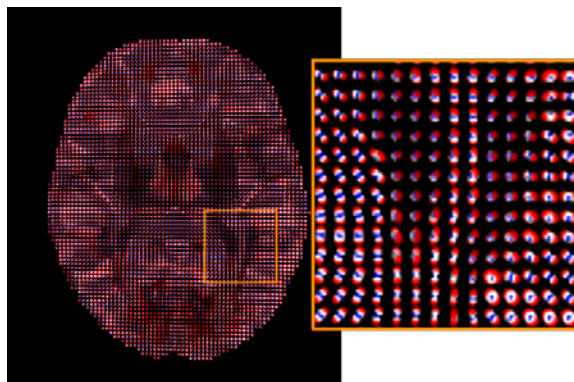
RESULT: Longitudinal DW-MRI Infant Atlas



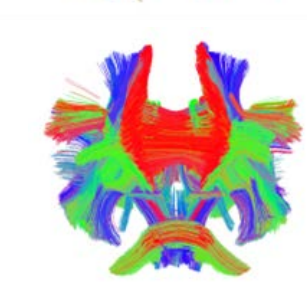
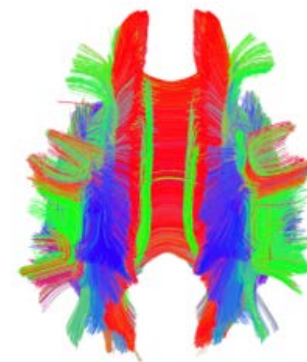
Baseline



Fractional Anisotropy

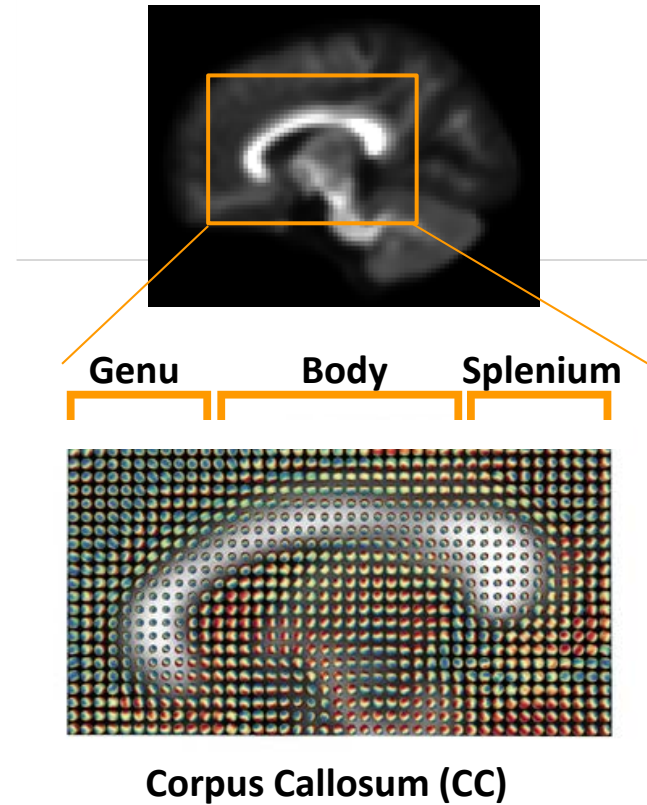
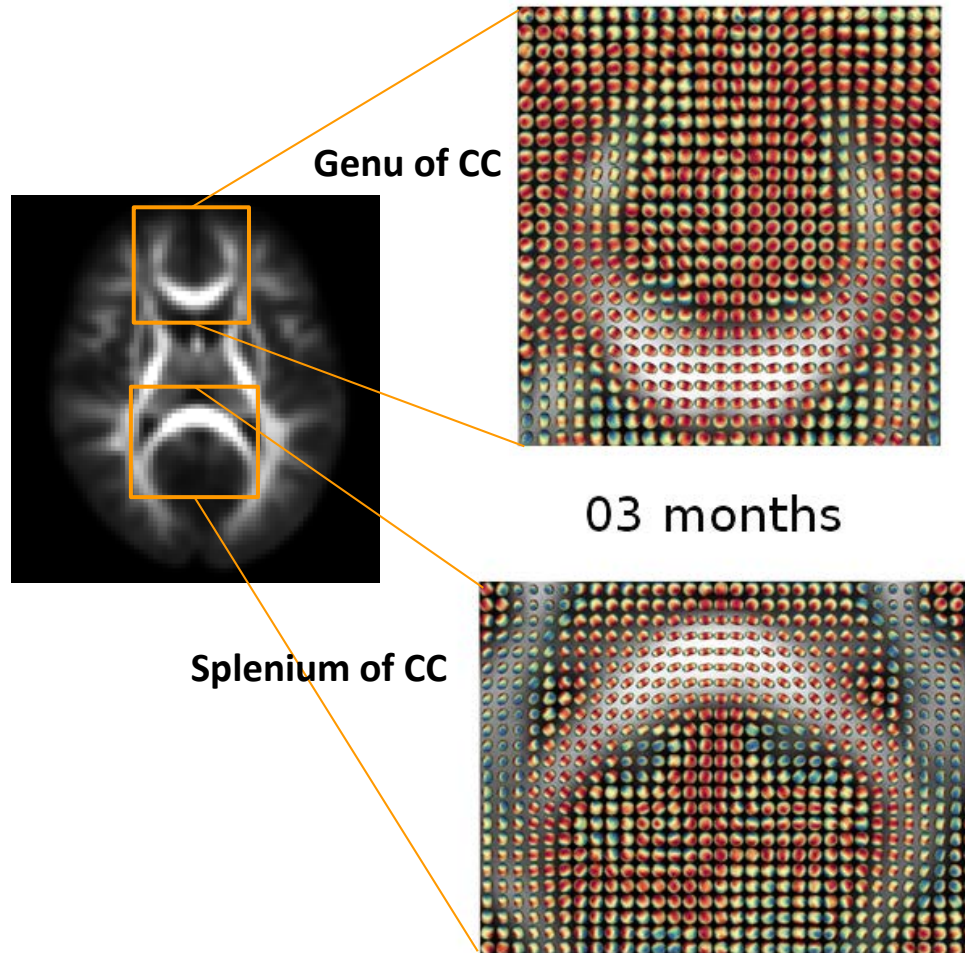


Diffusion orientation distribution function (dODF)

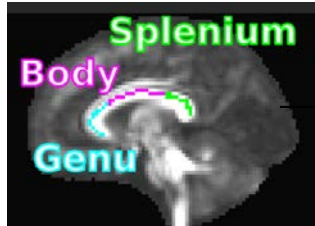


Tractography

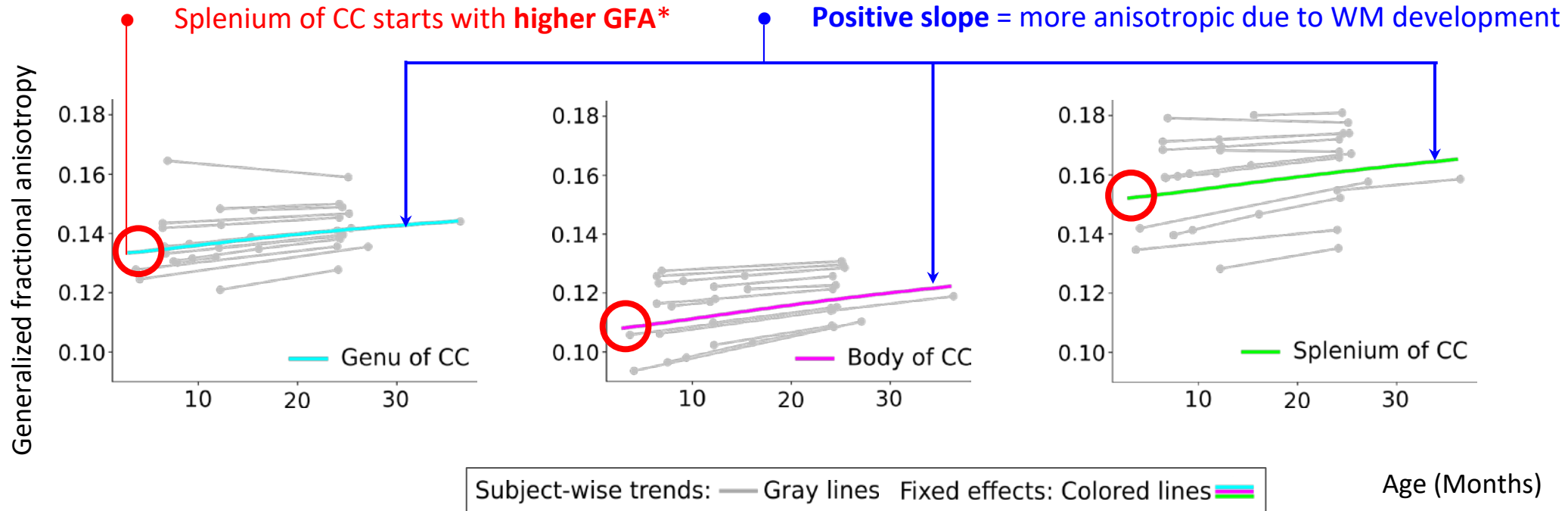
Analysis of corpus callosum



RESULT: Evaluation based on Longitudinal GFA Changes



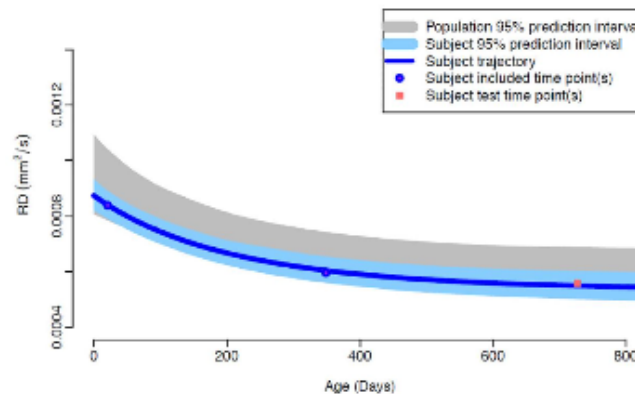
- Generalized fractional anisotropy (GFA) calculated for genu, body, and splenium of the corpus callosum



*Geng, X., et al., Neuroimage, 2012

Conclusion & Future Work

- **Done:** Framework to build a continuous longitudinal HARDI brain atlas based on statistics of dODF SH coefficients, applied to longitudinal data of healthy developing infants.
- **Goal:** To represent statistical normative model of dODFs over infant age.
- **Todo:** Explore nonlinear model.
- **Todo:** Modeling of population and subject specific confidence intervals (Sadeghi Neuroimage 2013).



This work was supported by the NIH grants R01-HD055741-12, 1R01HD089390-01A1, 1R01DA038215-01A1 and 1R01HD08812501A1. We are thankful for research discussions with Dr. Ragini Verma.

Hierarchical Multi-Geodesic Model for Longitudinal Analysis of Temporal Trajectories of Anatomical Shape and Covariates

Sungmin Hong, James Fishbaugh, Jason J. Wolff, Jane Paulsen, Martin A. Styner, Guido Gerig

- **Approaches so far:**

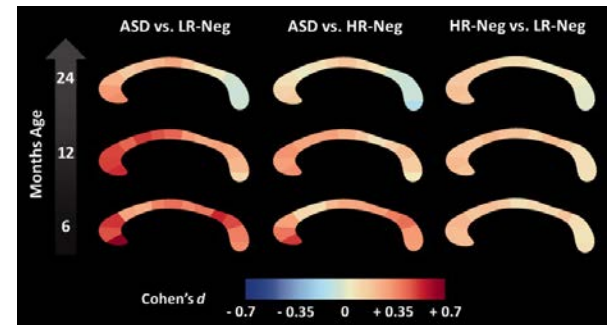
- Statistical shape modeling followed by generalized linear modeling with covariates and group testing (e.g. Wolff et al., Brain 2015).

- **New:**

- Novel hierarchical multi-geodesic model that can account for the effect of subject-specific covariates to the development (slope) of a shape change.

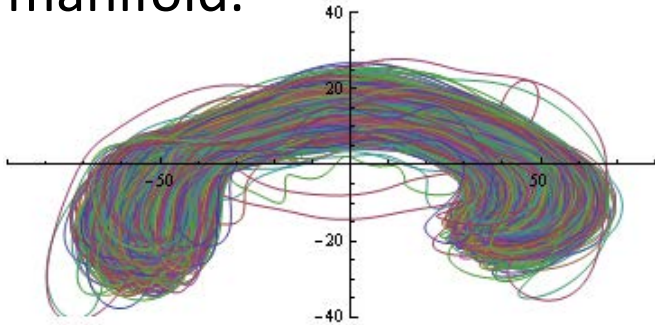
- **Goal:**

- Improved understanding of shape/covariate relationship.

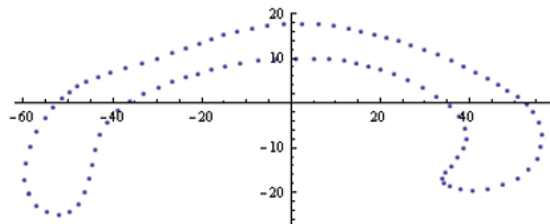


Shape representation and statistics

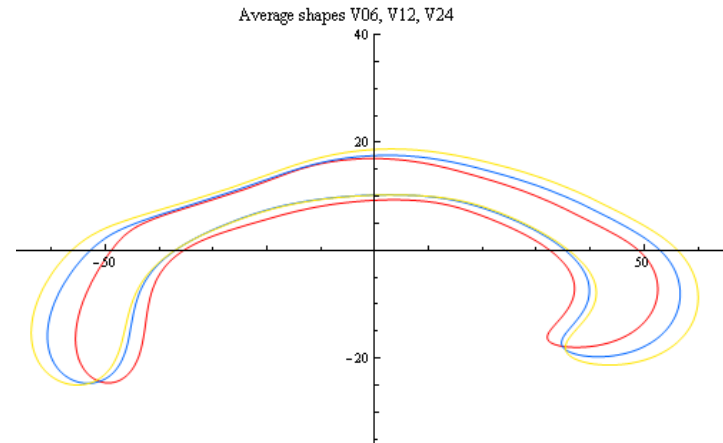
Shape space is non-Euclidean:
Geodesic model on Riemannian
manifold.



1040 corpus callosum shapes, ACE-
IBIS, sampled by boundary points.



Longitudinal Shape Change per
Subject



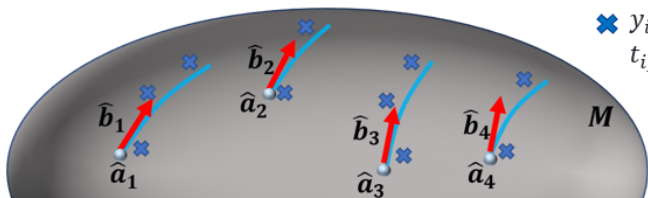
Hierarchical Model (“mixed effects model”, but covariate and time)

Estimate a subject-wise trend as a univariate geodesic model [1].

$$(\hat{a}_i, \hat{b}_i) = \operatorname{argmin}_{a_i, b_i} \sum_{j=1}^{N_{obs}^i} d^2(y_{ij}, \operatorname{Exp}(a_i, b_i t_{ij})),$$

$$Y_i = \operatorname{Exp}(\hat{a}_i, \hat{b}_i t)$$

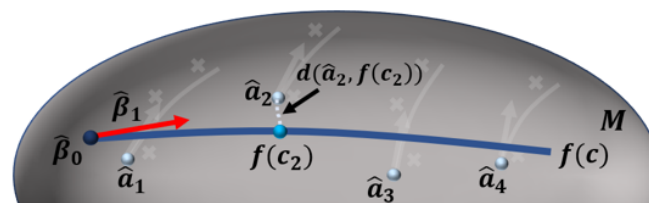
- Y_i : Subject-wise model
- ✕ y_{ij} : Observations
- t_{ij} : Observation Times



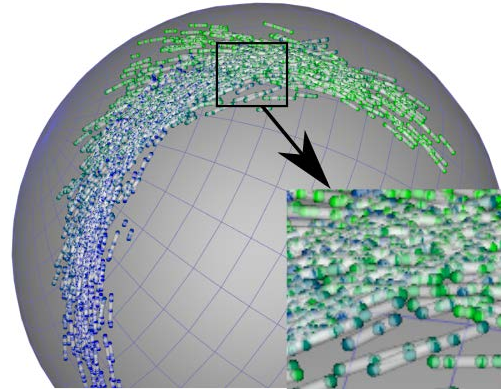
The intercept model $f(\eta)$ formulated as a multivariate geodesic model [2].

Models the effects of covariates to the baselines of subject-specific trends.

$$f(\eta) = \operatorname{Exp}(\beta_0, \beta_1 \eta_1 + \dots + \beta_{N_\eta} \eta_{N_\eta})$$

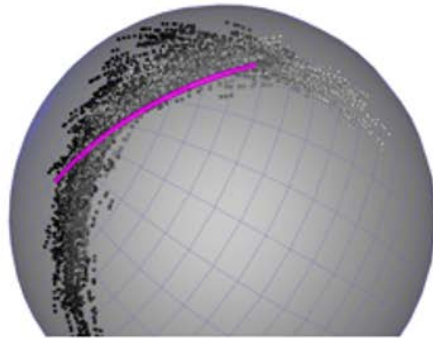


Synthetic Model: Statistical Analysis in Complex Shape Space

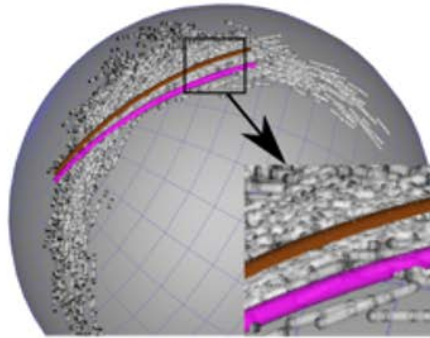


1000 subjects with 3500
points total,
covariate $c = [0..5]$

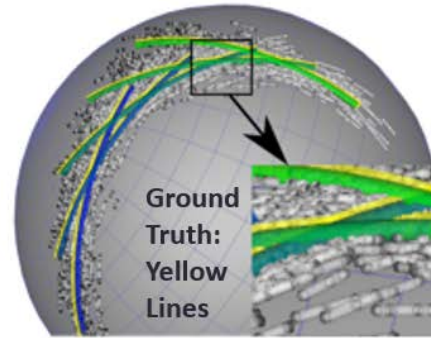
Lines: longitudinal subject
trends



Geodesic Model



Hierarchical Geodesic Model



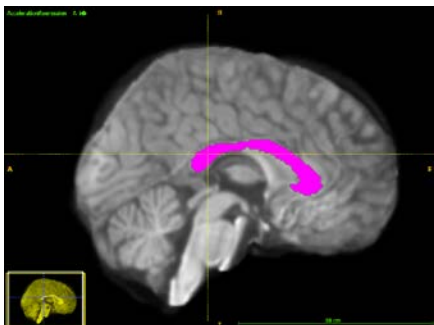
Proposed
Hierarchical Multi-Geodesic Model

Geodesic and Hierarchical
Geodesic models fail, cannot
account for covariate.

Proposed HMS: Proper
model of covariate and
individual trends

Study on ACE-IBIS Data (72 shapes, 24 ASD subjects)

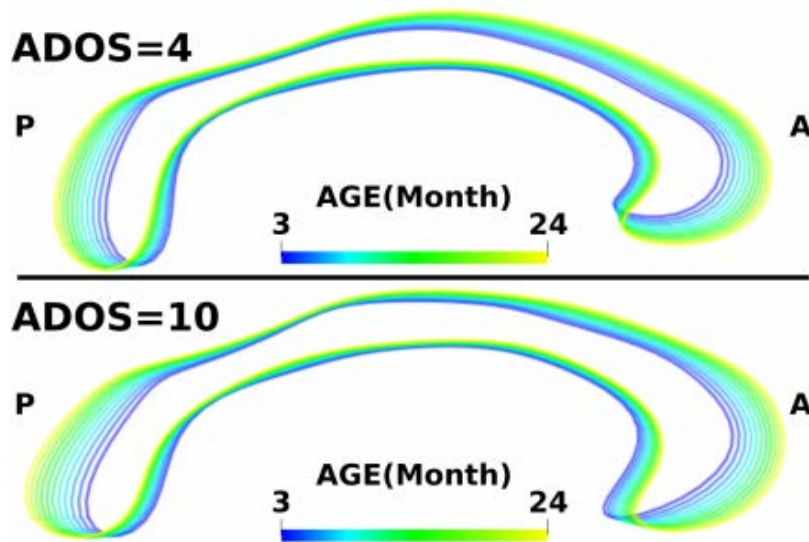
Corpus Callosum



Autism Diagnostic Observation Schedule (ADOS) Score

- Clinical test score on the behavioral and cognitive abilities
- 4 : Low ~ 10 : High

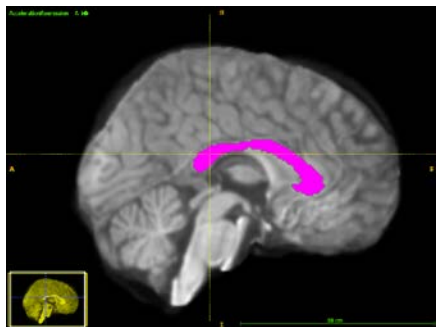
Shape Space : Scale x Kendall Shape - $\mathbf{M} = \mathbf{R} \times \mathbf{CP}^{k-2}$



Finding: Increased expansion of the anterior CC (genu and rostral body) over time for subjects with higher ADOS scores confirms expansion of CC in ASD.

Study on ACE-IBIS Data (72 shapes, 24 ASD subjects)

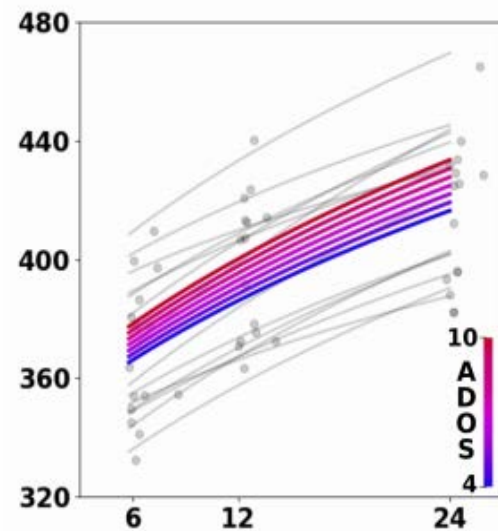
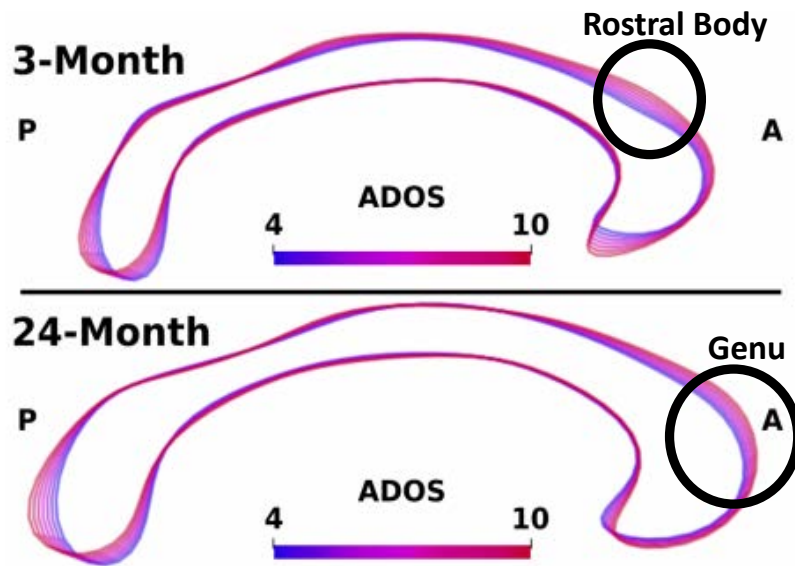
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